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(54) **SYRINGE WITH RETRACTABLE NEEDLE**

SPRITZE MIT EINZIEHBARER NADEL

SERINGUE AVEC AIGUILLE RETRACTABLE

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(56) References cited:
WO-A-90/07948 **CH-A- 669 910**
US-A- 4 838 869 **US-A- 4 994 034**
US-A- 5 049 133

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Description

[0001] The present invention relates to protection against accidental skin piercing by needles of used hypodermic syringes or medical samplers, or the like.

[0002] A used such needle poses a health hazard and considerable attention has been directed to reducing the hazard by disposal regimes and means of sheathing the needle tip after use. Also, numerous proposals have been made for automatic retraction of a needle after one use, but to date no-one appears to have put forward a practical proposal that is reliable and commercially viable to make, certainly not so that production costs are reasonable compared with the costs of existing products without needle retraction.

[0003] The present invention aims to improve practicality and viability in providing for reliable automatic needle retraction.

[0004] A large number of generally impractical or uncommercial prior proposals for hypodermic syringes with automatic needle retraction after use have been considered. They typically require the hollow needle to be fixed to a holder, commonly called a 'hub', and for such hub to be acted upon by a compression spring and by releasable detent or trigger means to release spring action and forcibly send the needle and its holder into the interior of the syringe or sampler, often into the plunger which will be hollow at least for that purpose. Generally, however, such provisions, including detent or trigger means, involve or are involved in an assembly attachable to the forward end of the syringe or sampler body and/or plunger, and/or in a part or parts fitted interiorly of the body, whether to the body or to the plunger or to both. Such provisions tend to be costly in themselves and in terms of assembly.

[0005] According to one aspect of this invention, a syringe body for a syringe device that is sterilisable and has a needle that is hollow for passage of contents of the syringe and is automatically retractable after use, the syringe body having an interior which comprises a main elongate cylindrical chamber adapted for taking a plunger in slidable sealing relation therein and a forward chamber extending distally from the main chamber beyond the end of the plunger movement and being adapted to house a spring to bias a holder for the needle, the syringe body having integrally moulded internal latching formations which are resiliently radially flexible and extend from the forward chamber towards and into the main chamber in directions generally parallel with longitudinal axis of the body, the integral internal latching formations serving in use for retaining the needle holder with the spring compressed inside the forward chamber in biasing the needle holder and for releasing of the needle holder for automatic retraction with the needle when the integral latching formations are radially outwardly deflected by the plunger at end of its movement, characterised by the syringe body being made from mouldable material moulded in one piece, and by the

integral internal latching formations being adapted for their radially outward deflection also to serve in releasing the syringe body from a moulding tool.

[0006] Such one-piece syringe device body compares favourably with prior reference WO90/07948 drawn specifically to our attention and showing in its Figures 2 and 3 internal latching formations of a syringe body that are not believed to be integrally mouldable by any known high speed/high volume injection moulding technique, specifically directed at an acute angle forwardly at transition to and towards its forward retraction spring housing chamber. US 4,994,034 also specifically drawn to our attention teaches a syringe device with a two-piece body having two main components that are separately moulded and sub-assembled, one affording a main plunger-accommodating chamber, and the other a forward retraction spring housing chamber with externally exposed latching formations to extend into the main chamber only after joining the two sub-assemblies, the latching formations being moulded on the forward chamber as external end formations thereof.

[0007] Integrally formed internal latching formations of one-piece bodies of this invention extend in the main chamber generally axially of the body to free ends having radially inwardly directed retaining formations, and are deflectable radially outwardly at their free ends both for release from a moulding tool, and for latching and release of the needle holder when directly engaged by said plunger. It is particularly advantageous for such latching formations to have substantially no deflection from axial parallelism with the body when in latching engagement with the needle holder.

[0008] A particularly convenient and advantageous one-piece body moulding has its forward or extension chamber of reduced sectional size compared with its main chamber (both preferably circular), and its latching formations extending internally substantially outward of registration with walling of the forward or extension chamber and further preferably evenly spaced about the axis of the needle. Preferably, each of the latching formations is at least partially within a respective one of localised outward formations of the main chamber adjacent the forward or extension chamber.

[0009] Compared with known prior proposals for hypodermic syringes with automatic needle retraction, a one-piece mouldable body part hereof represents substantial cost saving. This cost saving is increased when taken in conjunction with another aspect of this invention regarding standard practice for a syringe or sampler construction to include a hollow cylindrical body, a plunger slidable in the body, and a seal between the plunger and the body effective during sliding of the plunger to express syringe or sampler contents and/or to draw them in before sample expression. Hitherto, acceptedly satisfactory seals have been expensive items made of rubber.

[0010] According to this other inventive aspect, a syringe or sampler device body and slidable plunger con-

struction permits direct sealing between the plunger and the body, at least for operation only once but including a number of movements at least for initial entry, retraction to load, and pressing down to express. A suitable construction comprises a hollow cylindrical body, preferably circular cylindrical, and a plunger having at least a hollow head with a continuous outer rim to engage the body internally when slid therein; the plunger head rim, as made, being nominally of greater external size than internal size of the body, but being radially inwardly deformable by the body when slid therein, preferably with some temporary radially outward deformation of the body itself as the plunger head travels along the interior surface of the body.

[0011] Satisfactory mouldable synthetic plastics materials for the plunger head, preferably the entire plunger, and the body, can have different resistances to deformation, typically less resistance for the plunger head and more resistance for the body, at least for both as made. Inherently softer or more deformable and harder or less deformable materials for the plunger and the body, respectively, include, for the body, polypropylene, preferably nucleated (at least 0.2% preferably 0.3-0.5%) polypropylene having good clarity/transparency, strength and resistance to shrinkage/warpage during moulding (homopolymer having proved promising in prototypes); and, for the plunger, polyethylene, preferably high-density to give good seal performance and stability (Melt 7 having proved promising in prototypes). At least for such specified materials, the difference in nominal diameters of body interior and plunger head exterior can be up to 50 microns or more, preferably at least 25 microns.

[0012] Direct sealing between such a plunger head and body that is satisfactory for intended single use of a hypodermic syringe or sampler eliminates separately made and hitherto relatively expensive seal provisions.

[0013] However, the one-piece body aspect is viable with a piston that has a plunger head-to-body seal, particularly of much smaller size (typically a simple small 'O' ring) than customary in practice hitherto.

[0014] Use of a syringe or sampler body having a cylindrical main chamber for a plunger and a forward or extension chamber of reduced section extending therefrom for a needle retraction drive system is also capable of exploitation to greatly aid assembly in accordance with a further aspect of this invention. In this further aspect, a needle and immediately related retraction drive parts are placed in a guide that is slidable into the main chamber along its side walling to take the needle and its retraction drive parts up to the forward or extension chamber in axial registration therewith for insertion into that forward or extension chamber simply by being pushed off the guide.

[0015] Such simple assembly is readily suited to high volume automated production, and represents a significant improvement in assembly costs compared with prior known proposals.

[0016] Sealing is, of course, provided so that hypodermic syringe or sampler contents do not escape past the needle (rather than only through it), preferably with isolation also from needle retraction drive parts at least to save wastage of contents that would not be expressible from such a position, and a further aspect of this invention concerns such sealing.

[0017] That further aspect itself has, in reality, two aspects, namely use of a septum disc that is uninterrupted save for being pierced by the needle, whose passage therethrough can readily be assisted by application of lubricants, say at first piercing and/or afterwards (before sterilising) for retraction; and use of a sealing washer on a needle holder to seal between a main plunger chamber of a syringe or sampler body and a or said forward or extension chamber housing the needle and retraction drive parts before the syringe or sampler is used.

[0018] Lubrication may be by application of silicone material to the septum disc and/or the needle at first piercing, normally centrally and readily jiggled up separately from use of a guide as in the third-mentioned aspect, and afterwards to aid forced retraction. Needle holder sealing can be below a head of the holder or hub and even be aided by action of the latching means on the opposite side of the head.

[0019] Where, as is preferred, the plunger is hollow and serves to receive the retracted needle and associated retraction drive parts, such as spring and seals, it can be closed off by a thin rupturable disc or membrane that is subsequently ruptured by the rear end of the needle, or the needle holder (as is preferred using appropriate formations on its innermost end). Such disc or membrane may well be such as not to rupture when subjected only to maximum retraction spring force, i.e. so the plunger needs to continue to be pressed down at or even after the full effective expression stroke and spreading of latching provisions to release the needle and its holder. However, a disc or membrane that does rupture easily when subjected to the spring bias force is preferred.

[0020] Where the plunger has a deformable head rim that is compressed inwardly by the body for sealing purposes, the rupturable disc or membrane could be inward of the end of the plunger and its head rim, but by an amount less than the intrusion of the needle or its holder into the plunger accommodating chamber of the body. However, it is preferred to use a pre-tensioned membrane or film that is stretched before application to an extent beyond any compression effects on and from the plunger head rim in the body, i.e. to remain taut or at least not become slack. A satisfactory disc or membrane can be ultrasonically welded or heat welded (say impulse-heat welded) or solvent welded in place in a suitable jig. Suitable adhesives represent another alternative.

[0021] Deploying all of the above aspects and preferences of this invention together results in a hypodermic syringe set having no more than eight parts, namely

one-piece body with integral latching formations, a plunger, rupturable plunger end disc or membrane (if not integrally formed with the plunger), a needle, a needle holder or hub, a septum disc, a spring, and a needle holder or hub seal. Moreover, those parts are extremely easily assembled, and can meet all sealing, force and sterilisation requirements applied at least in the United Kingdom and by the World Health Organisation. Savings from omitting conventional large rubber plunger-to-body seals, and from easy assembly, enable a hypodermic syringe to be made economically, feasibly matching, even beating, manufacturing costs of conventional hypodermic syringes, certainly beating costs and likely performance for all prior retractable needle proposals we have seen to date.

[0022] It is desirable and preferred that a plunger receiving a forcibly retracted needle and retraction drive parts be trapped in the body when in that state, but be reasonably effectively prevented from reaching that state until after first use. Achieving same constitutes a fifth aspect of this invention when done by way of a spacer between the free end of the plunger and the corresponding end of the body, to avoid snap-in of complementary body and plunger formations. A preferred spacer has a part or parts that can temporarily latch to the body end and/or the plunger end, and further preferably has incorporated therein indication of sterilising have taken place, say as normally done by irradiation.

[0023] A suitable spacer can be of sheet form apertured to fit over the plunger stem and tearable for removal. A preferred sheet is of thick paper or cardboard and carries a spot or printing of radiation indicating type, say ink that changes colour. Tear perforations can be preformed, say at a return bend for the sheet to pass twice about the plunger stem beneath its head. One or each end of the sheet can be preformed with a fold that provides either or both of folding over an end flange of the body and the free end of the plunger.

[0024] It is also considered preferred and advantageous herein for lubrication of the needle to be done, or to be capable of being done, in a test operation, say using a blind cup with a septum disc closure carrying silicone and penetrated by the needle for prescribed pressure to be applied to the plunger for test purposes.

[0025] It will be appreciated that use as a sampler, i. e. for taking in patients' samples from veins etc (through the needle) is as feasible as a hypodermic syringe, then with needle retraction after expressing the sample. A double-ended needle can also allow use with pre-loaded drug capsules or cartridges. In both cases, a container (for blood etc sample or with drug etc) will be inserted into a body hereof instead of said plunger, and will have an end-seal that is broken or penetrated by the inner end of the double-ended needle. After loading or unloading the container and removing it from the body, said plunger can be reinserted into the body in order to operate the latching provisions and take the needle etc into its hollow interior. Such a plunger will not need, and pref-

erably will not have, either of a seal to the body or a rupturable closure of its end. Indeed, such a plunger, i. e. not for hypodermic syringe use and action, will preferably be clearly distinguished, say by colour.

[0026] It is further envisaged and preferred herein, and can be seen as a yet further aspect of invention, for there to be simple but effective positive retention of a retracted needle in the plunger interior, particularly by way of integrally mouldable and moulded internal formations. Specifically, the plunger can have interior effective capture formations that may be as simple as progressively tapered formations, such as fins, ribs or even flats. Such tapered formations will effectively grip thus slow and stop a hub or holder of the retracting needle and can be located so that a double-ended needle will not reach and penetrate outside the plunger.

[0027] Specific implementation for this invention will now be described, by way of example, with reference to the accompanying diagrammatic drawings, in which

Figure 1 is a longitudinal section through one embodiment;

Figures 2, 3 and 4 are similar sections showing before, during and after use states of a second embodiment;

Figures 5A,B,C are plan, edge-on, and installed views of a preferred spacer of folding sheet type;

Figure 6 shows a test procedure combined with needle lubrication;

Figures 7A,B show assembly of needle retraction drive parts;

Figure 8 is a detail concerning direct plunger-body sealing;

Figures 9A,B are side and head plan views of a needle holder;

Figure 10 is a detail transverse view concerning needle holder latching means of the body;

Figures 11 and 11A are part and detail longitudinal sectional views concerning samplers and cartridge drug dispensers.

[0028] In Figure 1, a syringe construction comprises a body 1 having a cylindrical bore 3 open to one end to receive slidably within it a hollow plunger 5 shown sealed to the bore 3 by a quite small 'O'-ring 7. The other end of the body 1 has an end wall provided with an axial through-hole 10 in an external axial extension 11 which is frustoconical to receive a needle sheath 13.

[0029] A hollow elongate needle 15 is carried by a holder or hub 17 of top-hat section at its inner end. The needle 15 goes from inside the bore 3, and passes through a septum seal 19 positioned at the inner end 20 of the body 1 and through-hole 10. That end 20 of the body 1 also has extending inwardly therefrom deflectable latch fingers 21 providing latching shoulders 25 and tapered actuating surfaces 27. The fingers 21 will spread radially outwardly when engaged by latch release surface 39 as will be described. An annular space

outwardly of the latch fingers 21 is shown filled with a soft rubber infill to occupy space which might otherwise be a source of air pockets. Acting between the end 20 of the body 1, actually seating on the septum seal 19, and an annular surface 31 of the holder or hub 17 is a compression spring 33 shown compressed with the needle 15 latched and held in its extended position by the fingers 21.

[0030] The end of the plunger 5 facing the needle 15 is shown closed by a plug 35 that seals relative to the interior of the plunger 5 and has latching fingers 37 engaging the end of the plunger 5. The ends of the fingers 37 are tapered to provide surfaces 39 that cooperate with the tapered faces 27 of the body fingers 21 when the plunger 5 is pushed into the body 1 to its maximum extent. The plug fingers 37 will then also flex radially inwardly, and the space between them is preferably also occupied by a soft rubber infill 30.

[0031] Displacement of the plunger 5 into the body 1 is shown hindered by a removable collar 42 disposed about the plunger 5 beyond the opposite end of the body 1. Shown inside the removable collar 41 are teeth 43 on the plunger 5 for engagement in complementary recesses 45 in the adjacent end of the body 1.

[0032] In use, as a hypodermic syringe, the needle protection sheath 13 is removed and material drawn into the body 1 in the usual manner by withdrawing the plunger, the required dosage being measured by suitable calibration on the syringe body after expulsion of any entrapped air in the usual manner. The needle 15 is then inserted into the recipient to be injected, and the contents discharged by displacing the plunger 5 down the body 1. There are two possibilities for activating retraction of the needle. One option is for the collar 41 to be removed before commencement of discharge and for the plunger to be moved through the discharge operation until the teeth 43 contact at 39, 27 and disengage the respective latching fingers 37, 21 so that the spring 33 urges the needle 15 to the left in Figure 1 and the plug 35 moves with the needle 15 into the plunger 5 which, in turn, becomes locked in the body 1 by cooperating engagement of the teeth 43 and recesses 45. Alternatively, the collar can be removed later, after injection use of the hypodermic syringe, and the needle withdrawal from the recipient before final movement of the plunger 5 to trigger retraction of the needle 15.

[0033] The materials employed in construction of the plunger can be low friction plastics, and it is readily possible to employ a compression spring 33 that will exert sufficient force to retract the needle 15 from recipient tissue as well as drive it within the plunger 5. A bleed hole 47 near the outer end of the plunger 5 avoids imposing undue restriction on movement of the plug 35 and needle 15 down the plunger 5.

[0034] Figures 2, 3 and 4 show as-made and sterilised (before packaging or after unpackaging, typically from a blister pack), loaded for injection, and retracted needle states, respectively, for another embodiment of this in-

vention. Reference numerals are generally advanced by one hundred, and differences are now described. Although not so shown in Figure 4, the septum disc 119 may travel with the needle 115 and take the spring 133 with it into the interior of the plunger 105 at automatic retraction.

[0035] As hindrance to premature needle retraction, the sleeve 41 of Figure 1 is replaced by an apertured and folded sheet tag 141, which may be of thick paper or card. Figures 5A,B,C show more detail including apertures 141A,B both to fit over the plunger 105 below its grippable end 105E when folded at 141C, and at 141D to aid removal by tearing, say aided by perforations at 141E. The doubled thickness between the plunger end 105E and the grippable end 101E of the body 101 prevents engagement of the rib 143 and the groove 145 (shown more rounded than toothing 43 and recessing 45 in Figure 1 for easier integral moulding and "bumping off" from the mould tools concerned). Folds at 141F,G enable sheet end portions 141H and 141K to engage over flanging of plunger and body ends 105E and 101E. Retention is aided by contact adhesive at 141L,M for edges of the plunger and body end flangings, or, and preferably, holding folds pinched together (not indicated in Figure 5C for clarity, though fold direction arrows do appear). The top of the sheet end 141K is a convenient place for imprinting or affixing a label carrying any data desired (such as date of manufacture, batch number, manufacturer, syringe capacity, needle size, etc) plus a tell-tale for sterilisation (say an ink that changes colour). The sleeve 41 could, of course, be similarly printed or labelled.

[0036] Figure 6 indicates a combined needle lubrication and test procedure, usually before sterilising but after fitting the tell-tale sheet tag 141, it uses a blind cup type of test cell 150, shown fitted with a rubber septum seal 151, and preferably of a depth capable of taking the whole exposed length of the needle 115 to aid lubrication simply by wiping the septum seal 151 with silicone lubricant. After such full penetration, the plunger 105 is pushed into the body 101, and pressure in the test cell is measured to reach a desired or required value, see sensor 152 and indicator 153. If all is well, the needle sheath 113 will be added and the product sterilised and packaged.

[0037] The embodiment of Figures 2 to 4 also has a further seal 160 engaged by the opposite end of the spring 133 from the septum seal 119. The seal 160 is of flat washer type and seals to taper 161 by coaction between the needle holder of hub 117 and the latch fingers 121, preferably to cause outer corner deformation of the seal 161 when the latch fingers 121 entrap the holder or hub 117 with the spring compressed in the body extension 111. The seals 119 and 160 both assist retention of contents of the body, but the seal 160 further isolates the body extension 111 and the spring 133 from body contents.

[0038] The whole needle and its holder or hub and re-

lated drive and seal assembly 115, 117, 119, 133, 160 is particularly readily assembled into the body extension chamber 111, see Figures 7A, B. In Figure 7A, the needle 115 is already in the holder or hub 117 and passes through the seal 160 and the spring 133 with its point about to pierce the septum seal disc 119 centrally, as can readily be jiggled up. After doing so, the whole is placed in a guide 170 of generally half (or less) cylindrical form with an inner radius or channel 171 matching to the needle holder or hub 117, spring 133 and seals 119, 160 and an outer radius presenting a surface 172 matching the interior of the main chamber of the body 101. The thickness of the guide 170 will thus correspond to the difference in diameters between the interior of that main chamber and the interior of the extension 111. It is then a simple matter to slide the loaded guide 170 along the body 101 until its end, or a nose part 173 matching the taper 161 (as shown), can go no further; and for the needle and drive assembly to be pushed off into the then-registering extension 111 until the latch fingers 121 (not shown for clarity) are spread and return to capture the holder or hub 117. If the extension 111 is not central, the latching fingers could be offset too, and the guide 170 match a particular orientation of the body 101 usually with the extension 111 uppermost. That would also involve a plunger requiring orientation. In practice, it is preferable to do no more than offset the needle in the hub or holder 117.

[0039] Figures 2 to 4 also indicate direct sealing between the plunger 105 and the body 101. An 'O'-ring seal as at 7 in Figure 1 represents a great saving compared with conventional large rubber mouldings for hypodermic syringes. However, integrally moulding a satisfactory seating that does not require adhesive or other bonding is difficult. Moreover, avoiding any separately made seal part at all represents a yet greater advance and saving. Suitable materials for head 105H of the plunger, actually the whole plunger in a practical integral moulding, and for the body 101, enable that greater advance and saving. A harder, less deformable and advantageously highly transparent material for the body 101 is nucleated homopolymer polypropylene, and a softer, more deformable and satisfactorily sliding and sealing material for the plunger head 105H is high-density Melt 7 polyethylene. Those materials allow a nominal oversize of the plunger head 105H relative to the interior bore of the main chamber of the body 101 of up to 50 microns resulting in small outward deformation of the body 101 as the plunger head slides along it, say as little as 2 microns or less, and a larger compressive inwards deformation of the plunger head 105H. Dashed lines on Figure 8 give some indications of such deformation (obviously excluding possible volumetric compression at least of the plunger head), but should not be taken as either to scale or accurate, as detail measurement has not been made.

[0040] It will be appreciated that compression of the plunger head 105H can increase its stiffness thus effec-

tiveness in flexing the latching-fingers 121 outwardly, that compression will not reduce internal diameter of the plunger 105 beyond clearance for the needle holder or hub 117 to pass it easily when a rupturable disc or membrane 136, preferably a pre-stretched film is ruptured, say by toothed rupture-aiding formations 117D on the end of the needle holder or hub 117 as shown in Figures 9A, B. Preferred stretched film (136) can be applied from sheet stretched in two directions, say using a suitable welding head pressed down towards a corresponding bank of upturned plungers (105). Figure 8 also indicates a preferred indenting 105D of the plunger 105 just rearward of its head 105H, which is practical using rearward tool parts that split longitudinally and also provide flanging at 105E, and a forward end tool part for the rim of the head 105H itself that will assure no tool break lines round that sealing rim.

[0041] It will be noted that the embodiment of Figures 2 to 4 does not show soft infill behind the latching fingers 121, though such can be provided if desired. In fact, the body 101 is highly advantageously formed with only localised outward formations affording accommodations for flexing of the fingers 121 when spread for automatic needle retraction, see at 90° intervals and referenced 126 in Figure 10. Suitable tooling for one-piece moulding of the body 101 will have a core part that has an outer retractable sleeve part with extensions to form the accommodations 126 and to permit both formation of the latch teeth 125 and tapered actuating surfaces 127, and core tool extraction by flexing the fingers 121 outwardly after retraction of the outer sleeve part, say using a pushed forward inner sleeve part. A particularly advantageous arrangement involves twisting during removal of the core tool.

[0042] It will also be noted that Figures 2 to 4 shown tapered inward formations 105F of the interior of the plunger 105, which may be fins or ribs or, and preferably, flats to grip the needle holder or hub 117 when it is forcibly retracted by action of the spring 133. As well as further assurance against any access to the needle 115 after automatic retraction, such provisions have particular value when this invention is applied to taking samples or to application of drugs etc pre-packed in cartridges as is becoming increasingly popular. For such applications, it is practical to utilise a double-sided needle and some suitable container for the sample or drug, see at 215 and 280 in Figure 11 also showing a pierceable septum type end seal 281 for such container.

[0043] Generally, sample-taking containers (280) can be of evacuated type so that they merely needed rupturing by the inner end of the needle (215) to draw a sample from its other end normally already inserted into a recipient to be sampled, or can be of piston type requiring piston withdrawal after such piercing by the inner end of the needle. For cartridge drugs etc, suitable containers (280) can have their own piston or piston attachment for expression after piercing by the inner end of a double-ended needle (280).

[0044] Figure 11 shows a soft flexible cover 282 for the inner end 215B of the needle 215, which cover 282 will be pushed down and ruptured by the inner end 215B of the needle 215 when the seal 281 is ruptured as the container 280 is loaded into the body 101 or pushed into its operative state. The cover 283 has an end rim 283R shown captured by a dished apertured retainer part 282 itself shown with an inner rim 284 by which it is snap-fitted onto a headed extension formation 285 of a modified needle holder or hub 217. Other fitting for the cover 282 can be used, say by way of stretching onto a ribbed or barbed upstand of the holder or hub 217. After a container 280 has been used, it will be removed by withdrawal from the inner end of the needle 215, and a modified plunger 205 will be used for automatic retraction of the needle 215 and its related drive parts effectively just as before. Sealing of such a plunger 205 to the body 101 will not be required, see clearance formations 205C in Figure 11A (and of which there could be many), nor will any rupturable closure of its end 205B. Such will distinguish the plunger 205 from those (5, 105) for hypodermic syringes, but colour can also be used and is preferred.

[0045] However, leaving the septum disc 119 at the end of the forward or extension chamber 111 by design (spring strength and stroke relative to needle length and lubrication and/or grip of the septum disc in the forward chamber) has the advantage of the used hypodermic syringe or sampler being sealed for disposal with the needle 115 irretrievably retracted into the plunger 105 then locked to the body 101.

[0046] It has proved feasible, even for prototypes, to achieve needle stability to the extent of resisting up to 9 kilograms point loading with an operative plunger pressure of only about 100 to 125 grams or so.

Claims

1. A syringe body (101, 111) for a syringe device that is sterilisable and has a needle (115) that is hollow for passage of contents of the syringe and is automatically retractable after use, the syringe body (101, 111) having an interior which comprises a main elongate cylindrical chamber (101) adapted for taking a plunger (105) in slidable sealing relation therein and a forward chamber (111) extending distally from the main chamber (101) beyond the end of the plunger movement and being adapted to house a spring (133) to bias a holder (117) for the needle (115), the syringe body (101, 111) having integrally moulded internal latching formations (121) which are resiliently radially flexible and extend from the forward chamber (111) towards and into the main chamber in directions generally parallel with longitudinal axis of the body, the integral internal latching formations (121) serving in use for retaining the needle holder (117) with the spring (133) compressed inside the forward chamber (111) in biasing the needle holder (117) and for releasing of the needle holder (117) for automatic retraction with the needle (115) when the integral latching formations (121) are radially outwardly deflected by the plunger (105) at end of its movement, characterised by the syringe body (101, 111) being made from mouldable material moulded in one piece, and by the integral internal latching formations (121) being adapted for their radially outward deflection also to serve in releasing the syringe body (101, 111) from a moulding tool.
2. Syringe body according to claim 1, wherein the latching formations (121) extend in the main chamber (101) to free ends having radially inwardly directed retaining formations (125).
3. Syringe body according to claim 2, wherein the latching formations (121) have substantially no deflection from axial parallelism within the body (101, 111) when in latching engagement with said needle holder (117).
4. Syringe body according to any preceding claim, wherein the forward or extension chamber (111) has a smaller section than the main chamber (101), and axially parallel extents of the latching formations (121) in the main chamber (101) are radially outward of walling of the forward or extension chamber (111).
5. Syringe body according to any preceding claim, wherein each of the latching formations (121) has a surface (127) by which its free end is deflected radially when engaged by a cooperating surface of said plunger (105).
6. Syringe body according to any preceding claim, wherein each of the latching formations (121) is at least partially within a respective one of localised outward accommodations (126) of the main chamber (101) adjacent the forward or extension chamber (111).
7. A syringe device comprising a syringe body according to any one of claims 1 to 6, and including a plunger (105) adapted for direct sealing (105H) between the plunger (105) and the main chamber (101) during sliding movement of the plunger (105) in the body.
8. Syringe device according to claim 7, wherein the plunger (105) has a hollow head with a continuous outer rim (105H) of greater nominal size than interior section of the main chamber (101), the main chamber (101) and the plunger head rim (105H) permitting deformation radially of the body (101).

9. Syringe device according to claim 8, wherein the plunger head and rim (105H) and walling of the main chamber (101) are both radially deformable, and the material of the plunger head and rim (105H) is more deformable than that of the main chamber walling (101). 5
10. Syringe device according to claim 7, 8 or 9, comprising a needle (115) and a spring (133) held in the forward chamber (111) by the latching formations (121), wherein the needle (115) has a septum disc seal (119) that is pierced by the needle (115) and is seated upon by the spring (133) in the forward or extension chamber (111). 10
11. Syringe device according to any one of claims 7 to 10, wherein a sealing washer (160) between the needle holder (117) and the spring (133) seats and seals between the needle holder (117) and entry (161) from the main chamber (101) to the forward or extension chamber (111). 15
12. Syringe device according to any one of claims 7 to 11, wherein said plunger (105) is hollow to accommodate the needle (115) and its holder (117) and any retraction drive parts (133, 119, 160) that move therewith, and is initially sealed at its end nearest the forward or extension chamber (111) by a rupturable closure member (136) that is ruptured by engagement with the inner end of the needle (115) and its holder (117). 20 25
13. Syringe device according to claim 12, wherein the closure member (136) is a pre-stretched film secured across the end of the plunger (105). 30 35
14. Syringe device according to claim 12 or claim 13, wherein the needle holder (117) has formations (117D) aiding rupture of the rupturable closure member (136). 40
15. Syringe device according to claim 12, 13 or 14, wherein the plunger (105) has interior tapering formations (105F) to slow, stop and grip the needle holder (117) in spring-driven automatic retraction. 45
16. Syringe device according to any one of claims 7 to 15, wherein the body (101) has formations (145) to cooperate with plunger formations (143) after automatic retraction so as to latch the plunger (105) in the body (101). 50
17. Syringe device according to claim 16, further comprising a removable spacer (141) between free ends of the body (101) and its plunger (105), the spacer (141) serving to prevent engagement of the formations (143, 145) by which the plunger (105) is latched on the body (101). 55
18. Syringe device according to claim 17, wherein the spacer (141) is of folded (141C) sheet material that is further folded over (141G, K; 141F, H) and adhered to the free end (105E) of the plunger (105) and flanging (101E) of the free end of the body (101).
19. Syringe device according to claim 17 or claim 18, wherein the spacer (141) carries at least a tell-tale (141K) for sterilisation having taken place.
20. A syringe device comprising a syringe body according to any one of claims 1 to 6, in combination with a container (280) insertable into the body (101), wherein the needle (215) is double-ended and its inward end (215B) serves to pierce a seal (281) of the container (280).
21. Syringe device according to claim 20, further comprising a plunger (205) adapted to be used after the container (280) is later removed in order then to release the latching provisions, wherein the plunger (205) does not make a seal to interior of the main chamber (101).
22. Syringe device according to claim 21, wherein the plunger (205) has an open end to receive the needle (215) and its holder (217).
23. A method of assembling a syringe device according to any one of claims 7 to 22, wherein the needle (115) and its holder (117) are installed in the body (101, 111) during manufacture of the device by assembly together with retraction drive parts including the spring (133) and any seals (119, 160) in a guide member (170) that is slidable in the main chamber (101) to bring said assembly into registration with entry to the forward or extension chamber (111), the assembly then being pushed off the guide member (170) and into the forward or extension chamber (111) with accompanying compression of the spring (133) until there is latching engagement of the needle holder (117) by the latching formations (121).

Patentansprüche

1. Spritzenkörper (101, 111) für eine sterilisierbare Spritzenvorrichtung, die eine Kanüle (115) aufweist, welche hohl ist, um den Inhalt der Spritze passieren zu lassen, und die nach der Verwendung automatisch zurückziehbar ist, wobei der Spritzenkörper (101, 111) einen Innenraum aufweist, der eine längliche zylindrische Hauptkammer (101), die so gestaltet ist, dass sie einen Kolben (105) aufnimmt, der sich in gleitend abdichtender Beziehung darin befindet, und eine Vorkammer (111) aufweist, die distal von der Hauptkammer (101) über den End-

- bereich der Kolbenbewegung hinaus verläuft und so gestaltet ist, dass sie eine Feder (133) aufweist, um gegen einen Halter (117) für die Kanüle (115) zu drücken, wobei der Spritzenkörper (101, 111) einstückig geformte, innere Arretiergebilde (121) aufweist, die elastisch radial flexibel sind und von der Vorkammer (111) zur Hauptkammer und in diese hinein in Richtungen verlaufen, die im Allgemeinen zur Längsachse des Körpers parallel sind, wobei die einstückigen inneren Arretiergebilde (121) im Einsatz dazu dienen, den Kanülenhalter (117) festzuhalten, wobei die Feder (133) im Innern der Vorkammer (111) zusammengedrückt wird und somit gegen den Kanülenhalter (117) drückt, und dazu dienen, den Kanülenhalter (117) zwecks automatischen Zurückziehens mit der Kanüle (116) freizugeben, wenn die einstückigen inneren Arretiergebilde (121) durch den Kolben (105) am Ende von dessen Bewegung radial nach außen verbogen werden, **dadurch gekennzeichnet, dass** der Spritzenkörper (101, 111) aus einem in einem Stück geformten formbaren Material gebildet ist, und dass die einstückigen inneren Arretiergebilde (121) für ihr radiales Verbiegen nach außen so gestaltet sind, dass sie weiterhin dazu dienen, den Spritzenkörper (101, 111) aus einem Formungswerkzeug freizugeben.
2. Spritzenkörper nach Anspruch 1, **dadurch gekennzeichnet, dass** die Arretiergebilde (121) in der Hauptkammer (101) in freie Enden auslaufen, die radial nach innen gerichtete Festhaltegebilde (125) aufweisen.
 3. Spritzenkörper nach Anspruch 2, **dadurch gekennzeichnet, dass** die Arretiergebilde (121) im Wesentlichen keine Abweichung von der axialen Parallelität innerhalb des Körpers (101, 111) aufweisen, wenn sie sich im Arretierkontakt mit dem Kanülenhalter (117) befinden.
 4. Spritzenkörper nach einem der vorhergehenden Ansprüche, **dadurch gekennzeichnet, dass** die Vor- oder Erweiterungskammer (111) einen kleineren Querschnitt aufweist als die Hauptkammer (101) und dass sich axial parallele Verlängerungen der Arretiergebilde (121) in der Hauptkammer (101) radial außerhalb der Wandung der Vor- oder Erweiterungskammer (111) befinden.
 5. Spritzenkörper nach einem der vorhergehenden Ansprüche, **dadurch gekennzeichnet, dass** jedes der Arretiergebilde (121) eine Fläche (127) aufweist, durch die ihr freies Ende radial verbogen wird, wenn es in Kontakt mit einer damit zusammenwirkenden Fläche des Kolbens (105) gelangt.
 6. Spritzenkörper nach einem der vorhergehenden
- Ansprüche, **dadurch gekennzeichnet, dass** sich jedes der Arretiergebilde (121) zumindest teilweise in jeweils einer außen gebildeten Aufnahme (129) der Hauptkammer (101) neben der Vor- oder Erweiterungskammer (111) befindet.
7. Spritzenvorrichtung, die einen Spritzenkörper nach einem der Ansprüche 1 bis 6 aufweist und einen Kolben (105) einschließt, der so gestaltet ist, dass während der Gleitbewegung des Kolbens (105) im Körper eine unmittelbare Abdichtung (105H) zwischen dem Kolben (105) und der Hauptkammer (101) gegeben ist.
 8. Spritzenvorrichtung nach Anspruch 7, **dadurch gekennzeichnet, dass** der Kolben (105) einen hohlen Kopf mit einem durchgehenden äußeren Rand (105H) aufweist, der eine größere Nenngroße als der Innenquerschnitt der Hauptkammer (101) besitzt, wobei die Hauptkammer (101) und der Kolbenkopfrand (105H) eine Verformung radial zum Körper (101) zulassen.
 9. Spritzenvorrichtung nach Anspruch 8, **dadurch gekennzeichnet, dass** sowohl der Kolbenkopf und -rand (105H) als auch die Wandung der Hauptkammer (101) radial verformbar sind und dass das Material des Kolbenkopfes und -randes (105H) stärker verformbar ist als das der Wandung der Hauptkammer (101).
 10. Spritzenvorrichtung nach Anspruch 7, 8 oder 9, die eine Kanüle (115) und eine in der Vorkammer (111) von den Arretiergebilden (121) gehaltene Feder (133) aufweist, **dadurch gekennzeichnet, dass** die Kanüle (115) mit einer als Scheidewand dienenden Scheibendichtung (119) versehen ist, die von der Kanüle (115) durchstoichen wird und von der Feder (133) in der Vor- oder Erweiterungskammer (111) in Position gehalten wird.
 11. Spritzenvorrichtung nach einem der Ansprüche 7 bis 10, **dadurch gekennzeichnet, dass** eine Dichtscheibe (160) zwischen dem Kanülenhalter (117) und der Feder (133) eingesetzt ist und eine Abdichtung zwischen dem Kanülenhalter (117) und dem Eintritt (161) von der Hauptkammer (101) in die Vor- oder Erweiterungskammer (111) bildet.
 12. Spritzenvorrichtung nach einem der Ansprüche 7 bis 11, **dadurch gekennzeichnet, dass** der Kolben (105) hohl ist, um die Kanüle (115) und ihren Halter (117) sowie vorhandene Rückziehantriebssteile (133, 119, 160) aufzunehmen, die sich zusammen mit ihm bewegen, und dass er zunächst an seinem der Vor- oder Erweiterungskammer (111) am nächsten befindlichen Ende mittels eines zerreißbaren Verschlusselementes (136) abgedichtet ist, das

durch den Kontakt mit dem inneren Ende der Kanüle (115) und ihrem Halter (117) zerrissen wird.

13. Spritzenvorrichtung nach Anspruch 12, **dadurch gekennzeichnet, dass** das Verschlusselement (136) eine vorgespannte Membran ist, die über das Ende des Kolbens (105) hinweg befestigt ist. 5
14. Spritzenvorrichtung nach Anspruch 12 oder Anspruch 13, **dadurch gekennzeichnet, dass** der Kanülenhalter (117) Gebilde (117D) aufweist, die das Zerreißen des zerreißenbaren Verschlusselementes (136) unterstützen. 10
15. Spritzenvorrichtung nach Anspruch 12, 13 oder 14, **dadurch gekennzeichnet, dass** der Kolben (105) innere spitz zulaufende Gebilde (105F) aufweist, um den Kanülenhalter (117) beim federgetriebenen automatischen Zurückziehen zu verlangsamen, anzuhalten und zu ergreifen. 15 20
16. Spritzenvorrichtung nach einem der Ansprüche 7 bis 15, **dadurch gekennzeichnet, dass** der Körper (101) Gebilde (145) aufweist, die nach dem automatischen Zurückziehen mit Kolbengebilden (143) ineinander greifen, um den Kolben (105) im Körper (101) zu arretieren. 25
17. Spritzenvorrichtung nach Anspruch 16, die weiterhin einen abnehmbaren Abstandshalter (141) zwischen freien Enden des Körpers (101) und seines Kolbens (105) aufweist, wobei der Abstandshalter (141) dazu dient, das Ineinandergreifen der Gebilde (143, 145) zu verhindern, durch die der Kolben (105) im Körper (101) arretiert wird. 30
18. Spritzenvorrichtung nach Anspruch 17, **dadurch gekennzeichnet, dass** der Abstandshalter (141) aus einem gefalteten (141C) Follenmaterial besteht, des weiterhin über das freie Ende (105B) des Kolbens (105) gefaltet (141G, K; 141F, H) und an dieses sowie an die Flanschung (101E) des freien Endes des Körpers (101) geklebt ist. 40
19. Spritzenvorrichtung nach Anspruch 17 oder Anspruch 18, **dadurch gekennzeichnet, dass** der Abstandshalter (141) mindestens eine Anzeigevorrichtung (141K) trägt, die anzeigt, dass die Sterilisation erfolgt ist. 45
20. Spritzenvorrichtung, die einen Spritzenkörper nach einem der Ansprüche 1 bis 6 in Kombination mit einem in den Körper (101) einsetzbaren Behälter (280) aufweist, **dadurch gekennzeichnet, dass** die Kanüle (215) doppelendig ist und ihr nach innen gerichtetes Ende (215B) dazu dient, eine Dichtung (281) des Behälters (280) zu durchstechen. 50 55

21. Spritzenvorrichtung nach Anspruch 20, die weiterhin einen Kolben (205) aufweist, der so gestaltet ist, dass er verwendet werden kann, nachdem der Behälter (280) später entfernt wird, um die Arretierelemente zu lösen, **dadurch gekennzeichnet, dass** der Kolben (205) keine Abdichtung gegen das Innere der Hauptkammer (101) bildet.
22. Spritzenvorrichtung nach Anspruch 21, **dadurch gekennzeichnet, dass** der Kolben (205) ein offenes Ende aufweist, um die Kanüle (215) und ihren Halter (217) aufzunehmen.
23. Verfahren zum Zusammensetzen einer Spritzenvorrichtung nach einem der Ansprüche 7 bis 22, **dadurch gekennzeichnet, dass** die Kanüle (115) und ihr Halter (117) im Körper (101, 111) installiert werden, indem sie während der Fertigung der Vorrichtung als Baugruppe zusammen mit den Zurückziehantriebsteilen einschließlich der Feder (133) und aller Dichtungen (119, 160) in ein Führungselement (170) eingegeben werden, das in der Hauptkammer (101) gleitbar ist, um die Baugruppe in den Eingang zur Vor- oder Erweiterungskammer (111) zu führen, die Baugruppe dann von dem Führungselement (170) weg und in die Vor- oder Erweiterungskammer (111) hineinzuschieben, wobei gleichzeitig die Feder (133) zusammengedrückt wird, bis ein Arretierkontakt des Kanülenhalters (117) mittels der Arretiergebilde (121) eintritt.

Revendications

1. Corps de seringue (101, 111) pour un dispositif de seringue qui est stérilisable et qui a une aiguille (115) qui est creuse pour le passage des contenus de la seringue et qui est automatiquement rétractable après utilisation, le corps de seringue (101, 111) ayant un intérieur qui comprend une chambre principale allongée cylindrique (101) adaptée pour qu'un piston (105) puisse y coulisser, de manière étanche, et une chambre avant (111) s'étendant de manière distale depuis la chambre principale (101) au-delà de la fin du mouvement du piston et étant adaptée pour loger un ressort (133) destiné à agir sur un support (117) pour l'aiguille (115), le corps de la seringue (101, 111) ayant des formations de verrouillage internes intégralement moulées (121) qui présentent une flexibilité radiale élastique, et s'étendent depuis la chambre avant (111) vers et dans la chambre principale dans des directions généralement parallèles à l'axe longitudinal du corps, les formations de verrouillage internes intégrales (121) servant lors de l'utilisation à retenir le support de l'aiguille (117) avec le ressort (133) compressé à l'intérieur de la chambre avant (111) en agissant sur le support de l'aiguille (117) et pour libérer le

- support de l'aiguille (117) pour la rétraction automatique avec l'aiguille (115) lorsque les formations de verrouillage intégrales (121) sont déviées radialement vers l'extérieur par le piston (105) à la fin de son mouvement, **caractérisé en ce que le corps de la seringue (101, 111) est fait à base de matériau, qui peut être moulé, moulé en une pièce, et en ce que les formations de verrouillage internes intégrales (121) sont adaptées à leur déviation radiale vers l'extérieure aussi pour servir à la libération du corps de la seringue (101, 111) à partir d'un outil de moulage.**
2. Corps de seringue selon la revendication 1, dans lequel les formations de verrouillage (121) s'étendent dans la chambre principale (101) jusqu'aux extrémités libres ayant des formations de retenue dirigées radialement vers l'intérieur (125).
 3. Corps de seringue selon la revendication 2, dans lequel les formations de verrouillages (121) n'ont substantiellement pas de déviation à partir du parallélisme axial à l'intérieur du corps (101, 111) lorsqu'elles sont en engagement de verrouillage avec ledit support d'aiguille (117).
 4. Corps de seringue selon l'une quelconque des revendications précédentes dans lequel la chambre avant ou la chambre d'extension (111) a une section plus petite que la chambre principale (101), et les longueurs axialement parallèles des formations de verrouillage (121) dans la chambre principale (101) sont radialement à l'extérieur des parois de la chambre avant ou d'extension (111).
 5. Corps de seringue selon l'une quelconque des revendications précédentes, dans lequel chacune des formations de verrouillage (121) a une surface (127) par laquelle son extrémité libre est radialement déviée lorsqu'elle est engagée par une surface de coopération dudit piston (105).
 6. Corps de seringue selon l'une quelconque des revendications précédentes, dans lequel chacune des formations de verrouillage (121) se trouve au moins partiellement dans un des emplacements respectifs situés à l'extérieur (126) de la chambre principale (101) adjacente à la chambre avant ou d'extension (111).
 7. Dispositif de seringue comprenant un corps de seringue selon l'une quelconque des revendications 1 à 6, et comprenant un piston (105) adapté pour une étanchéité directe (105H) entre le piston (105) et la chambre principale (101) au cours d'un mouvement de coulissement du piston (105) dans le corps.
 8. Dispositif de seringue selon la revendication 7, dans lequel le piston (105) a une tête creuse avec un bord extérieur continu (105H) d'une taille nominale supérieure à la section intérieure de la chambre principale (101), la chambre principale (101) et le bord de la tête du piston (105H) permettant la déformation radiale du corps (101).
 9. Dispositif de seringue selon la revendication 8, dans lequel la tête et le bord du piston (105H) et les parois de la chambre principale (101) sont tous les deux radialement déformables, et le matériau de la tête et du bord du piston (105) est plus déformable que celui des parois de la chambre principale (101).
 10. Dispositif de seringue selon la revendication 7, 8 ou 9 comprenant une aiguille (115) et un ressort (133) maintenus dans la chambre avant (111) par les formations de verrouillage (121) dans lequel l'aiguille (115) a un septum étanche en forme de disque (119) qui est percé par l'aiguille (115) et sur lequel le ressort (133) s'appuie dans la chambre avant ou d'extension (111).
 11. Dispositif de seringue selon l'une quelconque des revendications 7 à 10, dans lequel une rondelle d'étanchéité (160) entre le support de l'aiguille (117) et le ressort (133) s'appuie et crée l'étanchéité entre le support de l'aiguille (117) et l'entrée (161) depuis la chambre principale (101) vers la chambre avant ou d'extension (111).
 12. Dispositif de seringue selon l'une quelconque des revendications 7 à 11, dans lequel ledit piston (105) est creux pour recevoir l'aiguille (115) et son support (117) et toute pièce d'entraînement de rétraction (133, 119, 160) qui bouge avec ceci, et est initialement scellée à son extrémité la plus proche de la chambre avant ou d'extension (111) par un obturateur de rupture (136) qui se rompt par engagement avec l'extrémité intérieure de l'aiguille (115) et son support (117).
 13. Dispositif de seringue selon la revendication 12, dans lequel l'obturateur (136) est un film pré-étiré attaché de manière sûre en travers de l'extrémité du piston (105).
 14. Dispositif de seringue selon la revendication 12 ou la revendication 13 dans lequel le support de l'aiguille (117) a des formations (117D) aidant la rupture de l'obturateur de rupture (136).
 15. Dispositif de seringue selon la revendication 12, 13 ou 14, dans lequel le piston (105) a des formations intérieures en entonnoir (105F) pour ralentir, arrêter et agripper le support de l'aiguille (117) dans un mécanisme de rétraction automatique à ressort.

16. Dispositif de seringue selon l'une quelconque des revendications 7 à 15 dans lequel le corps (101) a des formations (145) pour coopérer avec les formations du piston (143) après rétraction automatique, de manière à verrouiller le piston (105) dans le corps (101). 5
17. Dispositif de seringue selon la revendication 16, comprenant en outre une entretoise amovible (141) entre les extrémités libres du corps (101) et son piston (105), l'entretoise (141) servant à éviter l'engagement des formations (143, 145) par lesquelles le piston (105) est verrouillé sur le corps (101). 10
18. Dispositif de seringue selon la revendication 17, dans lequel l'entretoise (141) est composée d'un matériau à feuillets plissés (141C) qui est ensuite replié (141G, K ; 141F, H) et collé sur l'extrémité libre (105E) du piston (105) et sur le collet (101E) de l'extrémité libre du corps (101). 15 20
19. Dispositif de seringue selon la revendication 17 ou la revendication 18 dans lequel l'entretoise (141) porte au moins un témoin (141K) du fait que la stérilisation a eu lieu. 25
20. Dispositif de seringue comprenant un corps de seringue selon l'une quelconque des revendications 1 à 6, en combinaison avec un conteneur (280) qui peut être inséré dans le corps (101), dans lequel l'aiguille (215) a deux extrémités et son extrémité intérieure (215B) sert à percer un joint d'étanchéité (281) du conteneur (280). 30
21. Dispositif de seringue selon la revendication 20, comprenant en outre un piston (205) adapté pour être utilisé après que le conteneur (280) est ensuite retiré de manière à alors libérer les provisions de verrouillage, dans lequel le piston (205) ne fait pas un joint d'étanchéité avec l'intérieur de la chambre principale (101). 35 40
22. Dispositif de seringue selon la revendication 21, dans lequel le piston (205) a une extrémité ouverte pour recevoir l'aiguille (215) et son support (217). 45
23. Méthode pour l'assemblage d'un dispositif de seringue selon l'une quelconque des revendications 7 à 22, dans laquelle l'aiguille (115) et son support (117) sont installés dans le corps (101, 111) pendant la fabrication du dispositif par assemblage, ensemble avec les parties d'entraînement de rétraction dont le ressort (133) et tout joint d'étanchéité (119, 160) dans une pièce guide (170) qui peut coulisser dans la chambre principale (101) pour faire se positionner ledit assemblage dans l'entrée de la chambre avant ou d'extension (111), l'assemblage étant expulsé de la pièce guide (170) et propulsé dans la chambre avant ou d'extension (111) avec la compression d'accompagnement du ressort (133) jusqu'à ce qu'il y ait un engagement de verrouillage du support de l'aiguille (117) par les formations de verrouillage (121). 50 55

Fig. 1

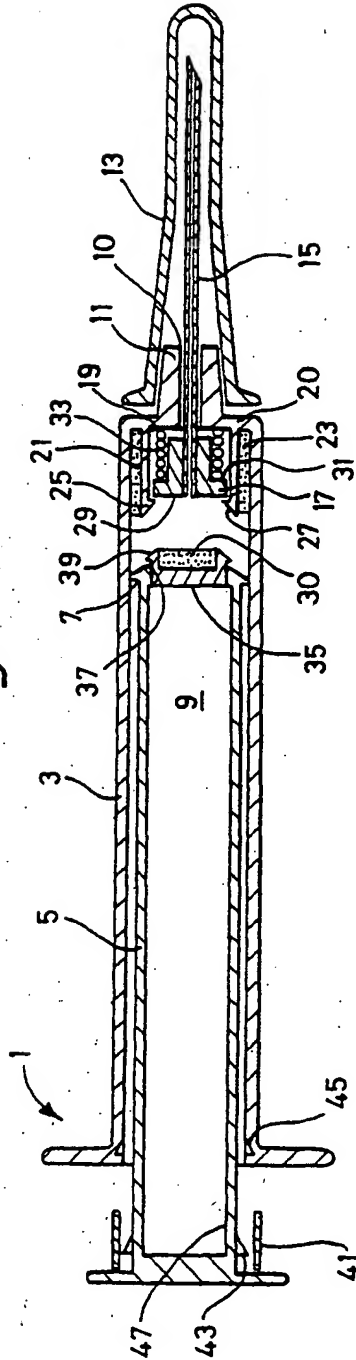


Fig. 2

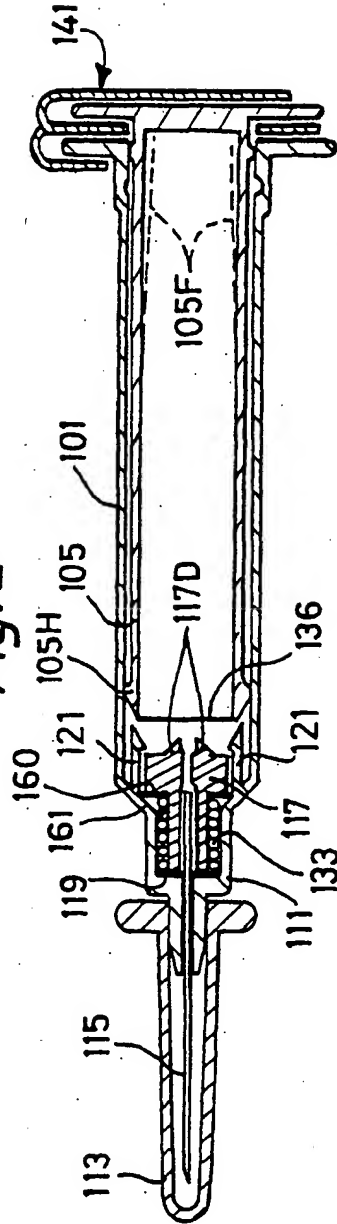


Fig. 3

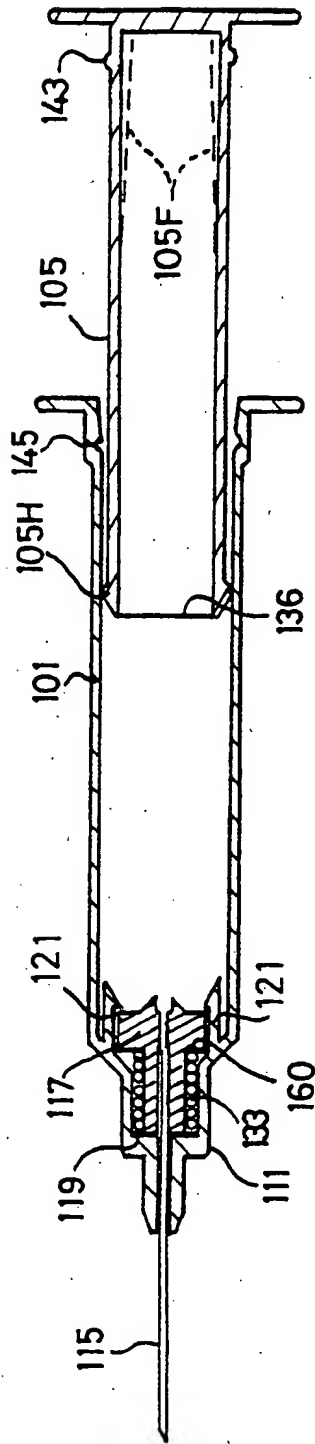


Fig. 4

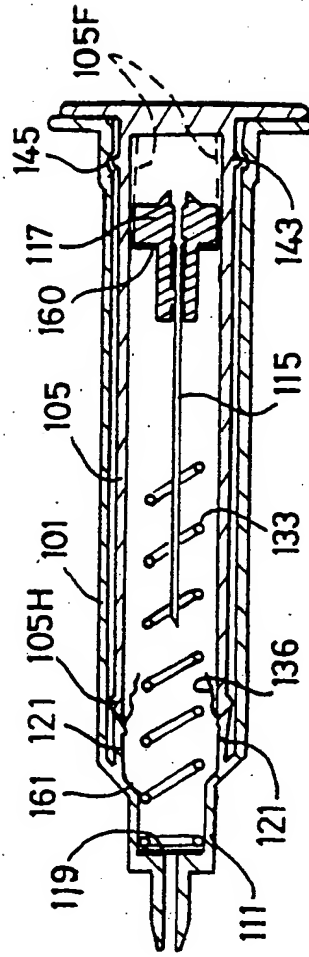


Fig. 5A

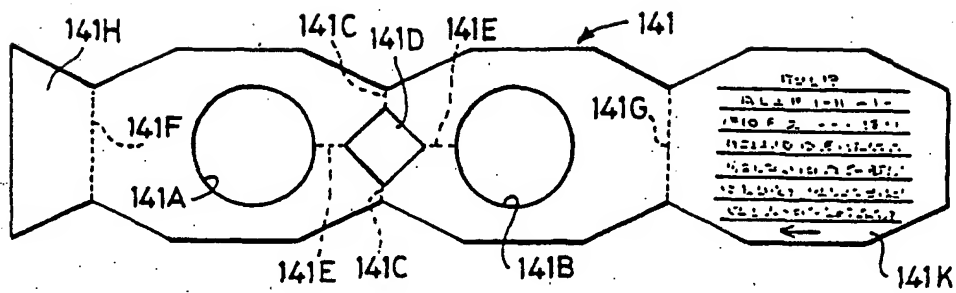


Fig. 5B

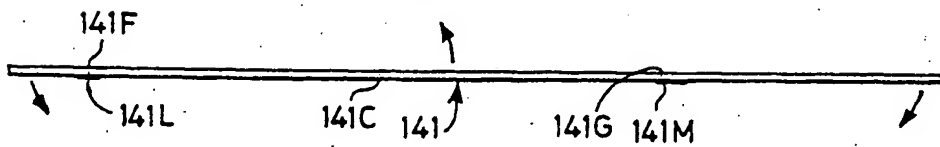


Fig. 5C

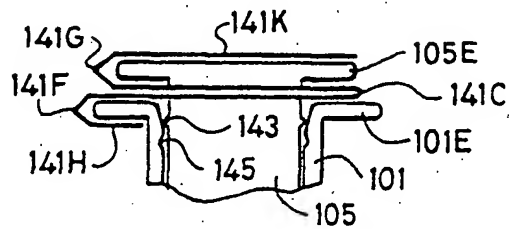


Fig. 6

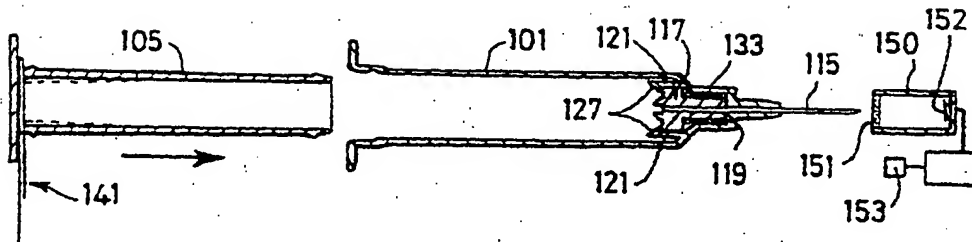


Fig. 8

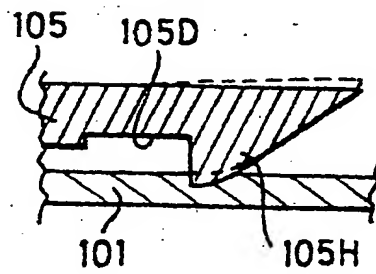


Fig. 10

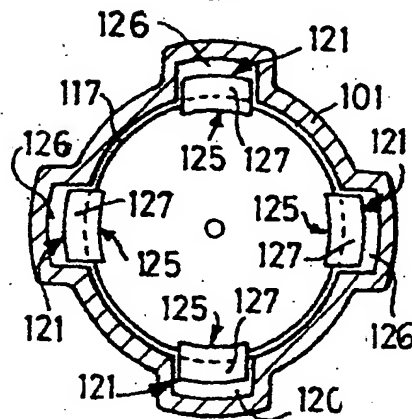


Fig. 7A

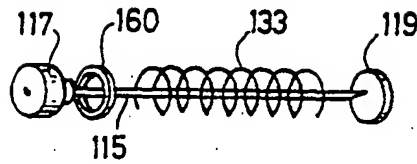


Fig. 7B

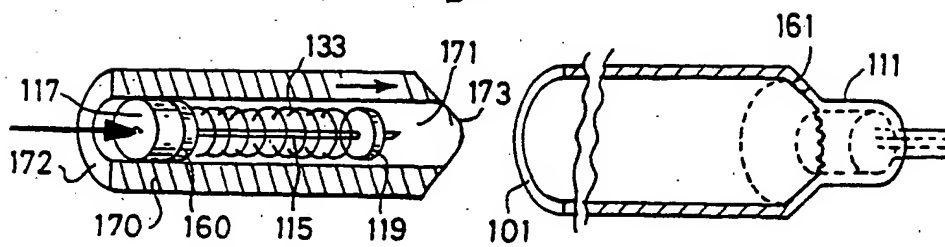


Fig. 9A

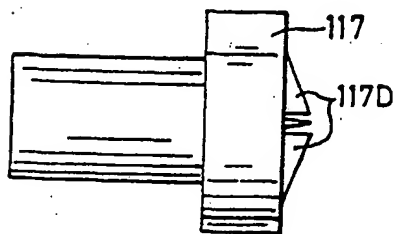


Fig. 9B

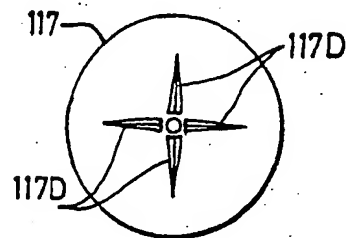


Fig. 11

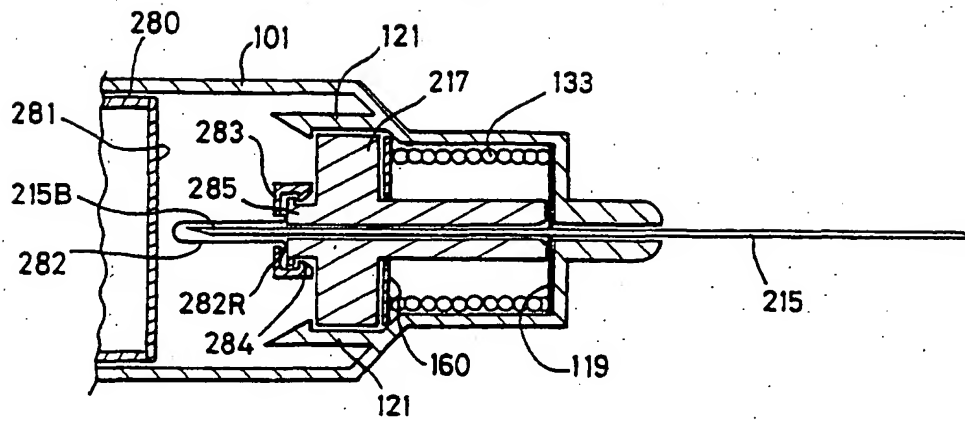
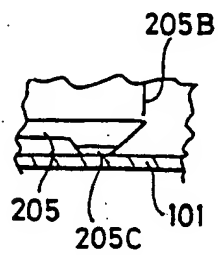


Fig. 11A



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